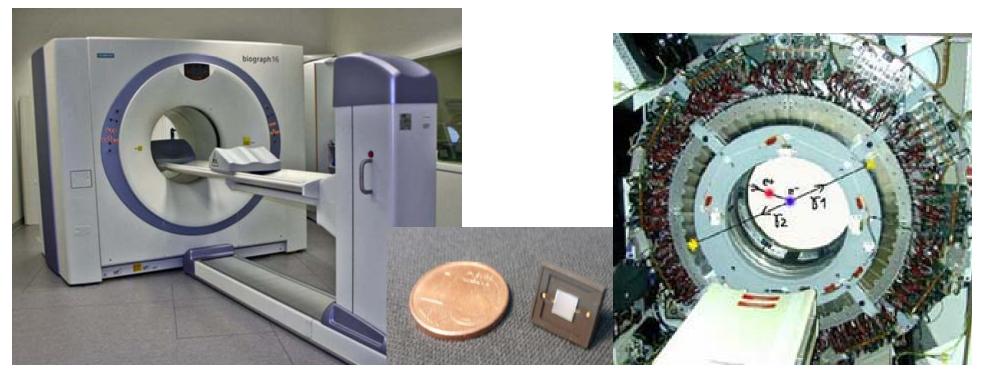


PET Design: Simulation Studies using GEANT4 and GATE

- Status Report -

Martin Göttlich

DESY



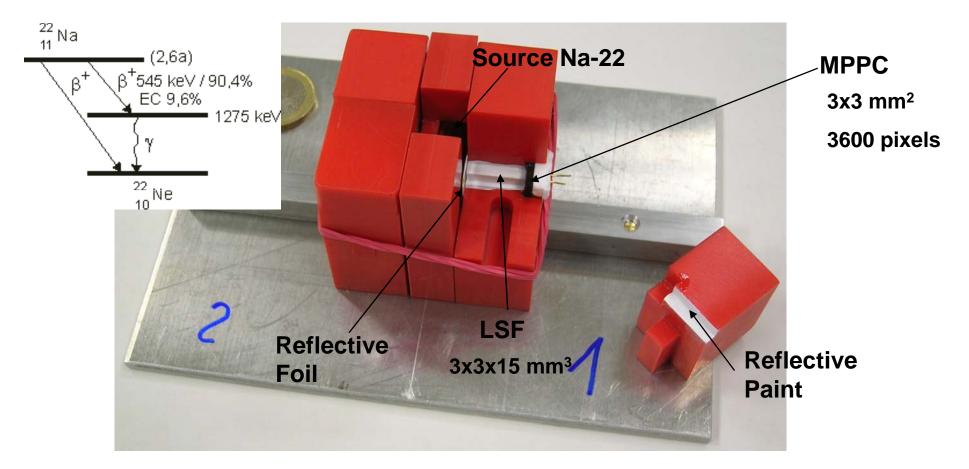


Outline

- Measurements
- Single crystal studies (GEANT4)
- PET scanner (GATE)



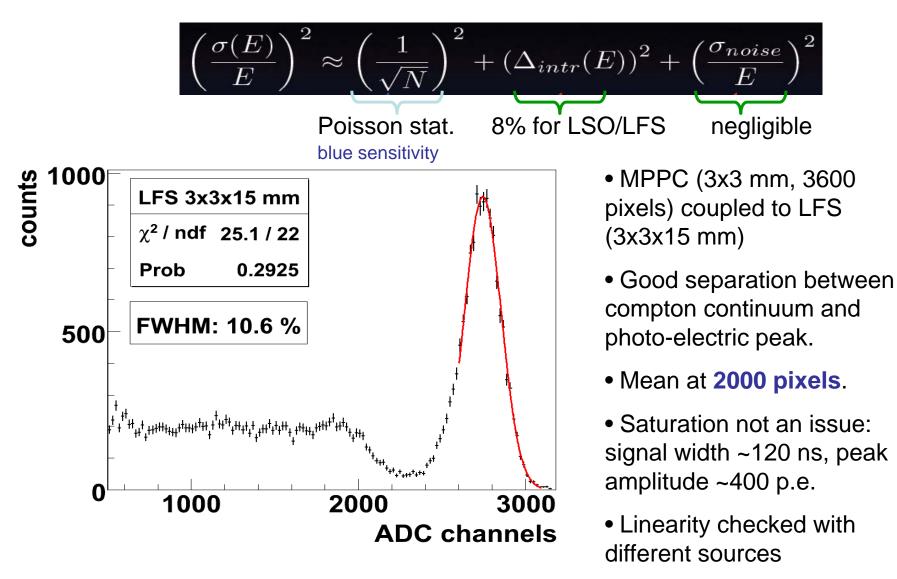
Experimental Setup



- MPPC and crystal well aligned, optical photons well contained, high reproducibility
- Reaching energy resolutions of 10-11 % FWHM (LSO and LSF)

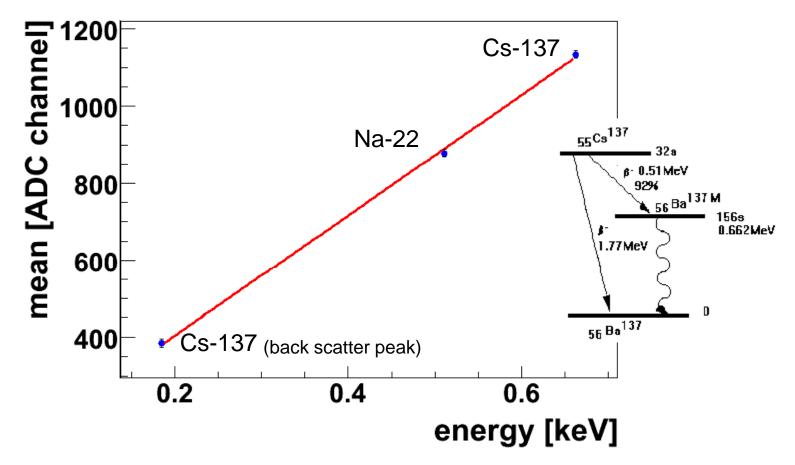


Energy Resolution





Linearity



Linearity confirmed in the energy region of interest.



Simulation Studies

Single Crystal + MPPC

- Detailed studies to optimize single crystal dimensions
- GEANT4 simulation
- Good description of the measurements in terms of energy resolution and photon yield.

PET System

- Design of a full PET system
- Spatial resolution (image reconstruction using FBP)
- Optimize crystal dimensions (DOI)
- **GATE** (GEANT4 Application for Tomographic Emission) toolkit based on GEANT4
- First results very promising.



Single Crystal + MPPC GEANT4 Simulation

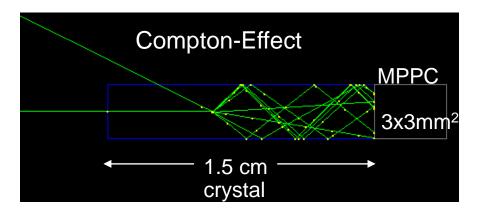
Important parameters:

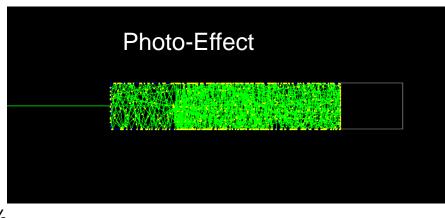
- LSO/LSF: scintillation yield (23k), refraction index (1.82), emission spectrum, absorption length (50m)
- Optical grease BC-630 (10µm): refraction index (1.5)
- MPPC: quantum efficiency
- Teflon wrapping: **reflectivity** (0.98), **refraction index** (1.34)

Compare to measurements:

- number of pixels
- signal width
- signal shape

30 reflections: P(absorbed)=45% (98% reflectivity)

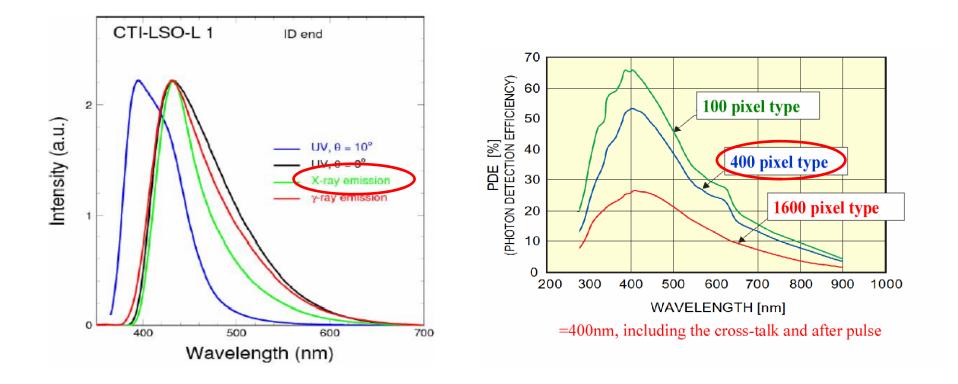




(LY: 100 photons/MeV)



Scintillation Yield and Photon Detection Efficiency



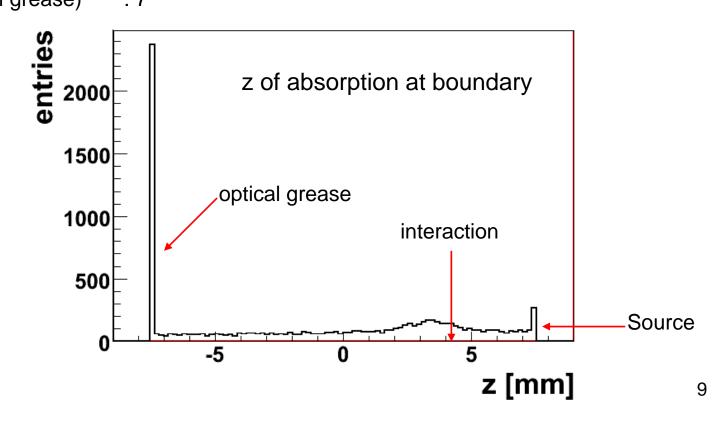
Incorporated published distributions.



A Single Event

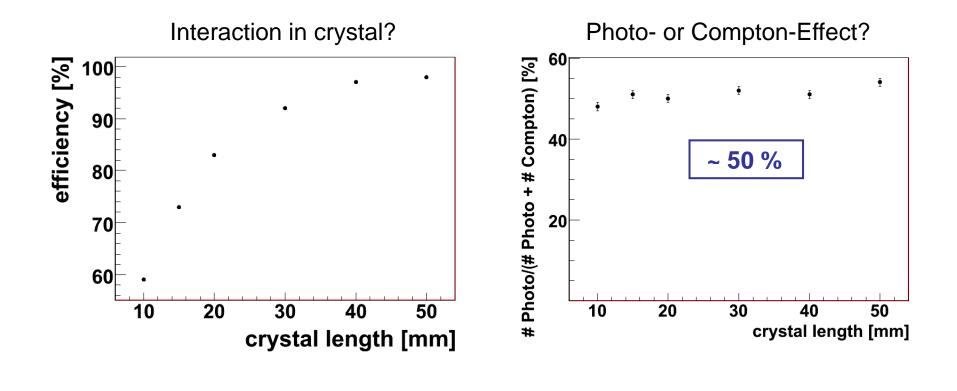
Number of photons produced : 10940Absorbed in the crystal: 9Absorbed at boundary: 9013Detected: 1911Leakage (optical grease): 7

Crystal length: 1.5 cm Reflectivity (Teflon): 90 %





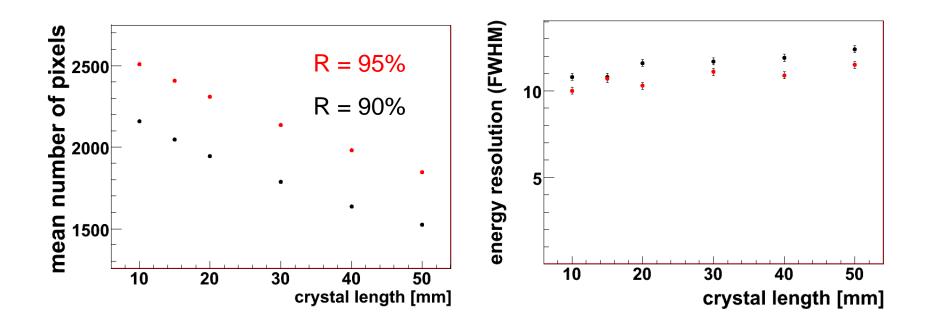
Efficiency



→ 5 cm > total length > 3 cm



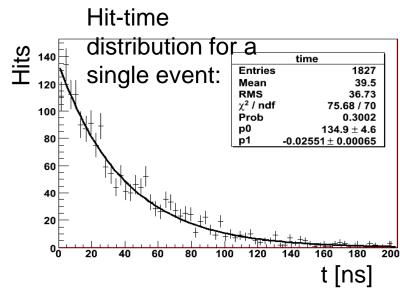
Energy Resolution



- Energy resolution is slightly decreasing for longer crystals due to absorption in the Teflon wrapping.
- The larger the reflectivity the smaller the effect.

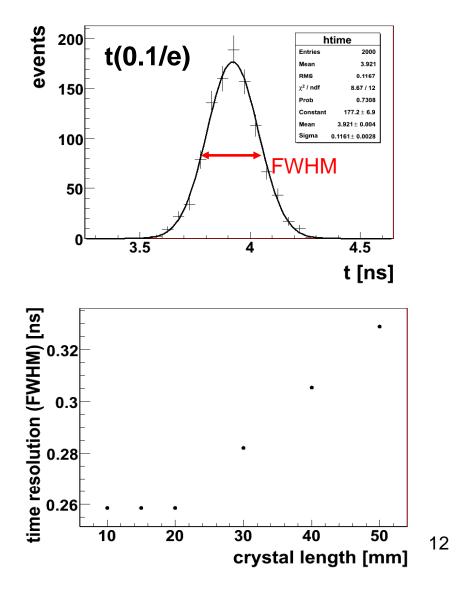


Time Resolution



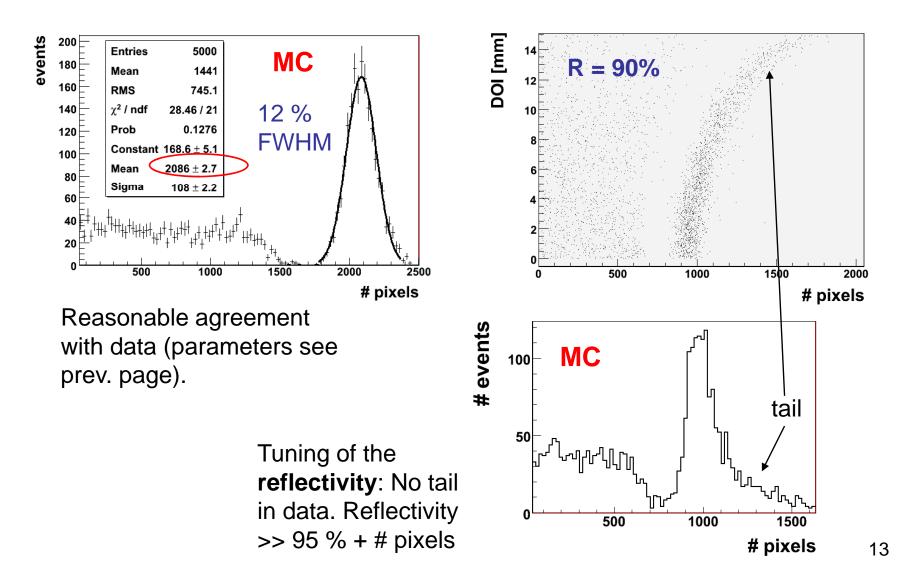
Triggering at low threshold, i.e. the very first photons which arrive:

Crystal length has only a small influence on the timing.





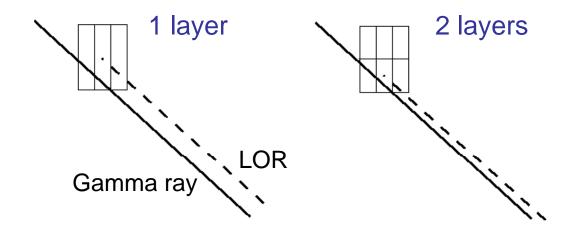
Measurements vs. Simulation





Crystal Length and DOI

Depth of interaction (DOI) information improves resolution considerably.

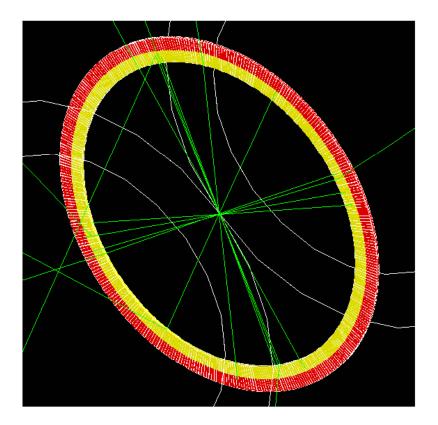


Simulation of a full PET scanner

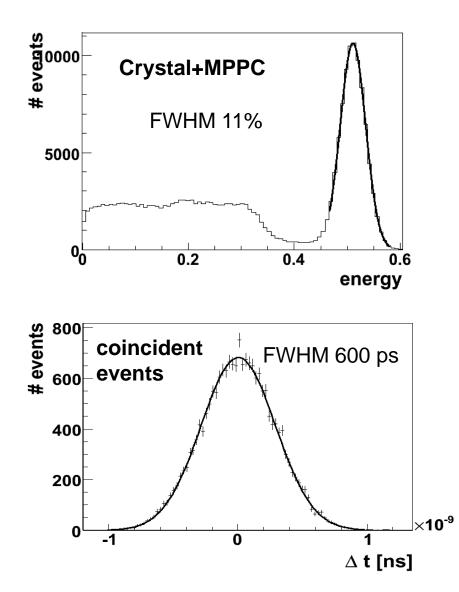


PET System - GATE

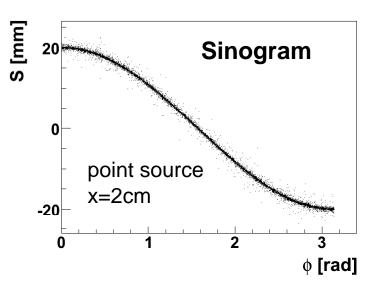
- Simulation of a full PET system to optimize camera design (high granularity, DOI, TOF).
- Image reconstruction using Filtered Back Projection (STIR)
- Determination of spatial resolution in compliance with NEMA NU 2-2007 standard*.
- Dead material, movement, noise, dead time, dose, phantom, scan time, efficiency
- Simulation of a simple PET system: 2x387 crystals (LSO, 3x3x15 mm³)







Tune energy and time resolution of single crystal+MPPC element according to measurements.



next steps: granularity, FBP (STIR)



Conclusions and Outlook

- Simulation: Tools are ready. More detailed studies follow. Emphasis on simulation of full PET scanner.
- Build and test prototype.



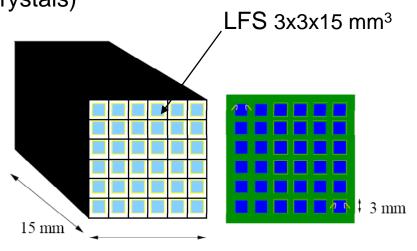
BACKUP FOILS



Design Criteria

Camera design (matrix of crystals, each crystal read out individually by an MPPC) guided by the following criteria:

- spatial resolution (DOI: two layers of crystals)
- time resolution
- efficiency
- exposure to radiation, scan-time
- costs



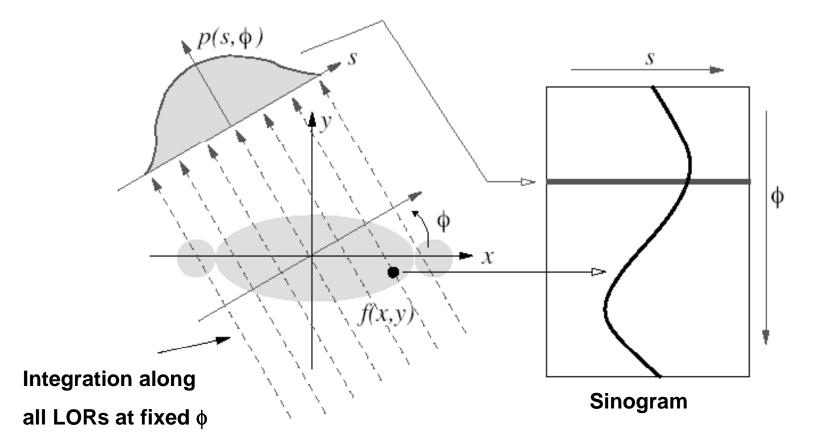
20 mm

Prototype:

- Two matrices of 6x6 crystal double-layers
- Study uniformity of channels, multi-channel r/o, calibration
- Image reconstruction of a point source

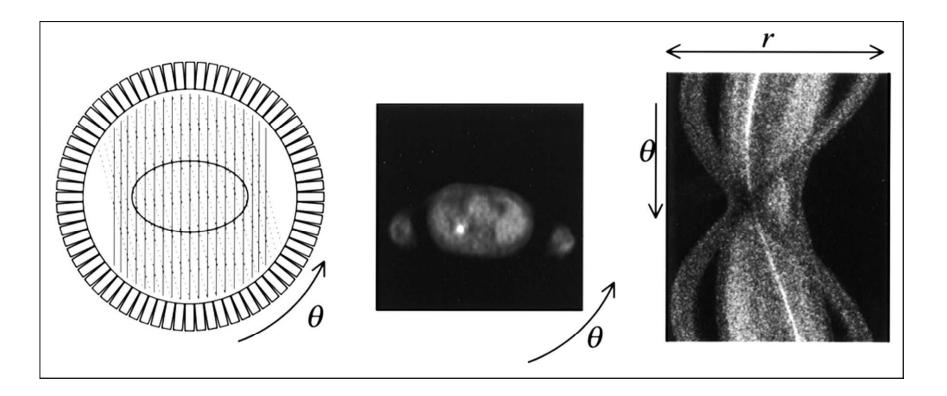


Sinogram





Sinogram - Example



Each point in the sinogram corresponds to a LOR.

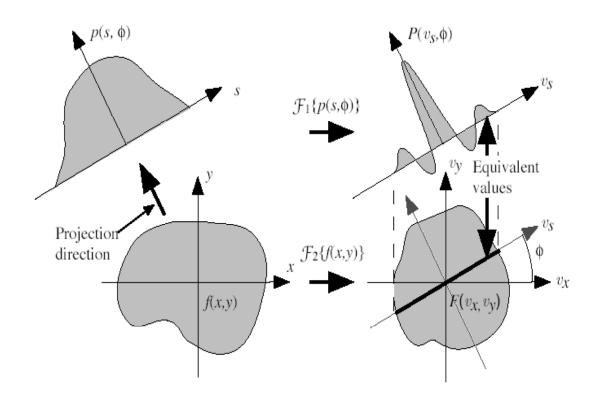


Filtered Back Projection

(Analytic 2D image reconstruction)

Imaging system: **p** = **Hf** + **n**

p: observation, **H**: system model, **f**: image, **n**: error (Radon transform closely related to Fourier transform.)



Solution: unfolding, inverse problem ill-posed, regularization

2D central-section theorem:

The Fourier transform of a 1D projection is equivalent to a section at the same angle through the center of the 2D Fourier transform of the object.

Ramp-filter:

$$p^{F}(s,\phi) = \mathcal{F}_{1}^{-1}\{ |v_{s}|\mathcal{F}_{1}\{p(s,\phi)\} \}$$



A Commercial Example

GEMINI TF PET/CT (Philips)

- diameter of 90 cm, axial field of view of 18 cm
- 4 x 4 x 22 mm³ LYSO (lutetium-yttrium oxyorthosilicate) crystals
- coincidence timing resolution: 585 ps
- resolution near the center: 4.8 mm (FWHM)
- single high-quality image: 1-2 min
- whole-body scan: **10-30 min** (depending on patient size)
- available for \$1.85M

